

Comparative Study of Surface Displacement in Discs Following Chemonucleolysis and Lasernucleotomy

Hans-Paul Kutschera, MD,^{1*} Werner Lack, MD,¹ Martin Buchelt, MD,¹ and Rudolf Beer, Dr TECHN²

¹Department of Orthopaedics, University of Vienna, A-1090 Vienna, Austria

²Technical University of Vienna, A-1090 Vienna, Austria

Background and Objective: Dynamic changes of the dorsolateral protrusion site have been postulated to play an important role in the therapeutic effect of lasernucleotomy and chemonucleolysis. Basic biomechanical effects of the annulus after lasernucleotomy and chemonucleolysis are investigated.

Study Design/Materials and Methods: This study evaluates the in vitro bulging of lumbar discs comparing lasernucleotomy and chemonucleolysis. The horizontal displacement at the ventral and dorsolateral surface of 20 cadaver discs were tested by application of a continuously increasing axial deformation before and after therapy. The increase in horizontal displacement due to this longitudinal deformation was measured.

Results: Bulging was significantly lower at the puncture site of the chemonucleolysis needle as well as at that of the laser trocar. Significantly reduced bulging of the annulus was observed after chemonucleolysis. Slightly increased bulging was observed after lasernucleotomy in the total posterior region. There was a tendency to decreased stiffness after chemonucleolysis and a significantly decreased stiffness after lasernucleotomy.

Conclusions: The in vitro effect of lasernucleotomy seems to be based on reduction of the stiffness by distributing the load all over the annulus, whereas chemonucleolysis reduces bulging. Lasers Surg. Med. 22:275–280, 1998. © 1998 Wiley-Liss, Inc.

Key words: pressure measurement; disc protrusion; percutaneous disc surgery; disc deformation

INTRODUCTION: TREATING PROLAPSED DISCS

Percutaneous treatment of disc protrusions was diversified by introduction of new methods. Besides the semiinvasive methods of treatment of prolapsed discs, chemonucleolysis and percutaneous nucleotomy [1–3], lasernucleotomy is now established as a third method [4–12]. Up to now, most retrospective and prospective clinical investigations refer to chemonucleolysis as a standard procedure [1,13–16]. Therefore, novel methods are compared to chemonucleolysis [17]. In a randomized multicenter study, automated percutaneous discectomy, strongly propagated during the

1980s, yielded less satisfying results than chemonucleolysis [18]. In contrast, lasernucleotomy, the most recent method, showed satisfying results in several studies [5,6,19]. However, there are no reports in the literature on experimental comparative studies. Experimental studies measuring in-

Contract grant sponsor: Scientific Board of the Lord Mayor of Vienna.

*Correspondence to: Hans-Paul Kutschera, Department of Orthopaedics, University of Vienna, Währinger Gürtel 18-20, A-1090 Vienna, Austria.

Accepted 2 April 1997

tradiscal pressure in chemonucleolysis as well as in lasernucleotomy showed a decrease in intradiscal pressure for both methods [6,20–22]. Up to now, the biomechanical changes of the outer posterior annulus have not been investigated in a comparative study. The posterolateral deviation by disc protrusion is responsible for the compression of the adjacent dorsal neurogenic structures [3,23]. Therefore, we investigated the outer deviation of the disc before and after lasernucleotomy and chemonucleolysis, respectively, and compared the effects of both methods on the dorsal annulus area.

MATERIALS AND METHODS

Disc Specimens

Twenty segments of cadaver discs from human lumbar spines were prepared for both methods. Segments consisting of two vertebral bodies and one disc each were resected and investigated within 48 hours after resection. The specimens were stored at -4°C and warmed up toward room temperature prior to investigation. The segments were dissected from the adjacent soft tissue, longitudinal ligament, processus transversus, processus spinosus, and pedicle. The vertebral bodies were cut parallel to the horizontal plane of the intervertebral disc so that the axial force could be distributed perpendicularly over the disc. For reproducibility of the investigations, we chose only macroscopically unchanged discs. All discs with spondylosis, spondylarthrosis, and small intervertebral space ($<0.6\text{ mm}$) were excluded. Intact discs were determined by two repeated load cycles before treatment. Discs without reproducible pretreatment measurements were classified as pathologic discs and excluded from the study. All discs in the study showed comparable values before treatment. Of these 20 lumbar segments, we treated 10 discs each by lasernucleotomy and by chemonucleolysis, respectively.

Laser

For this series of experiments, we used a $2.12\text{ }\mu\text{m}$ Holmium-YAG laser (Coherent/USA) with a pulse duration of $250\text{ }\mu\text{sec}$. For nucleus vaporisation we used a $360\text{ }\mu\text{m}$ fiber (Clarius/USA) with a trokar-permitting ablation as well as suction. Ablation was performed under continuous rinsing with saline solution and suction at a flow of 10 ml per minute. In all cases the laser fiber was positioned dorsolaterally on the side of sensor 3. Energy was increased stepwise by 1 kJ

and was interrupted for 30 seconds after each step (range $1\text{--}10\text{ kJ}$). Ablation was performed at an energy of 1.4 J and a frequency of 10 Hz up to 10 kJ total energy, in accordance with the clinical instructions for lasernucleotomy [10–12].

Chemonucleolysis

Chymopapain (Chymodiactin®, Boots) was diluted in 2 ml aqua bidest. In our experimental setup, we used $4,000$ units chymopapain per nucleus. To ensure a constant effect of chymopapain, the measurements were performed routinely starting immediately after and up to 2 hours after injection, according to the instant effects described in prior publications [15,24].

Experimental Setup

The biomechanical testing machine controlling the axial displacement consisted of an axial fixing device for the vertebral segment permitting the application of a continuously increasing deformation force. Axial shift was introduced (0.5 mm/turn) and the axial forces were measured in Newton (N) by an integrative measurement device (Technical University of Vienna). Three sensors were positioned ventrally and on both sides dorsolaterally of the disc. The displacement produced by the lateral surface deformation of the annulus was measured by the sensors each connected to a candelabra beam supplied with a strain gauge half bridge (Fig. 1). The measurement device for the lateral deformation was connected to an elastic candelabra beam, and dislocation of the tip of the strips could be measured with an accuracy of $\pm 0.01\text{ mm}$. The data measured were recorded by a data logger (Schlumberger, Vienna). The measurement device could be fixed by a magnetic rack at a variable position and height according to the dimensions of the test specimens. The test specimens were fixed with claw plates and bone cement (Sulfix®) perpendicular to the axis to avoid the occurrence of horizontal shear forces.

Measurement

The experiment was performed stepwise under deformation control up to a corresponding total load of 400 Newton (average velocity: 2.5 N/sec). Before the treatment two load cycles were done to ensure reproducible data. Bulging of the disc was measured as mm value (Fig. 2). We compared the horizontal displacement due to analogous load cycles before and after therapy, calculated in mm lateral per mm axial decrease of the longitudinal disc deformation. Elasticity, the re-

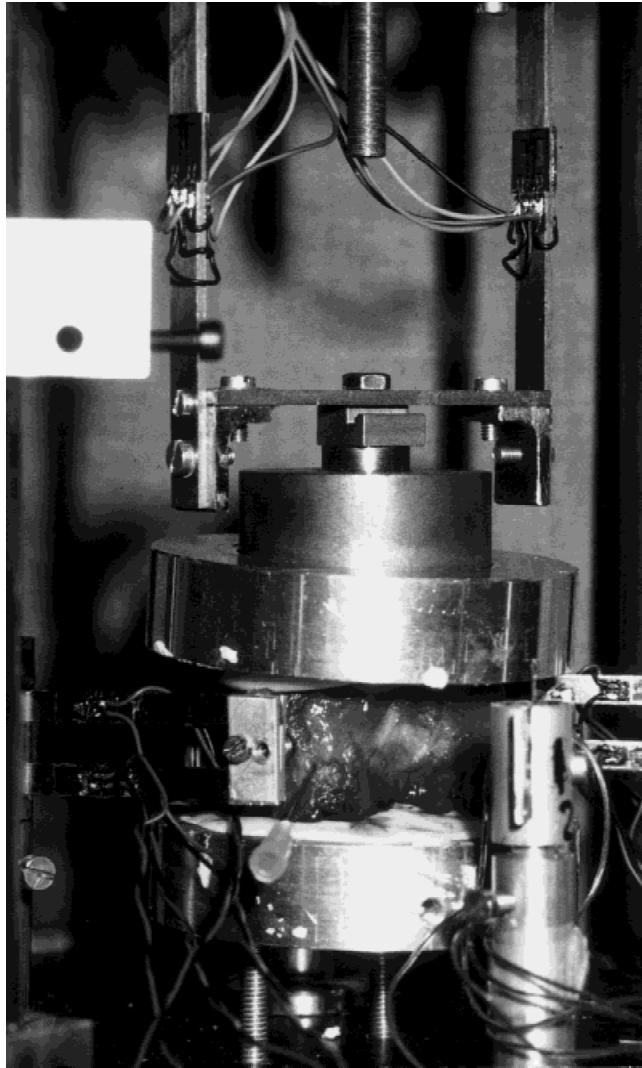


Fig. 1. Measurement device with candelabra beam in dorso-lateral position of the disc. Vertebral segment fixed with claw plates and bone cement.

ciprocal value of stiffness, was measured in Newton per μm decrease (Fig. 3).

Statistics

Multivariant analysis using statistical methods to analyze the basic effect was performed. Statistical analysis was performed using Student's t-test and significance was assumed at P values < 0.5 .

RESULTS

Preoperative Bulging

The preoperative measurements of the external annulus bulging exhibited no statistical differ-

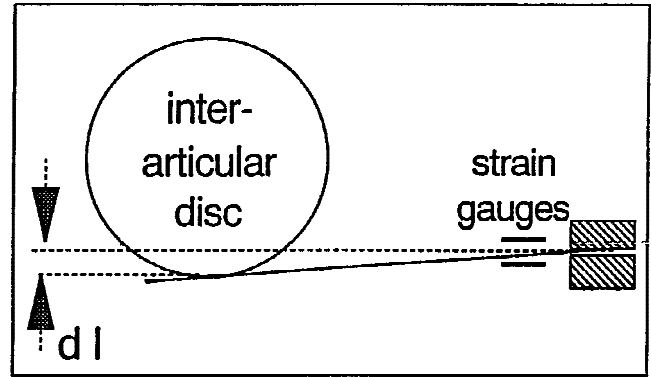


Fig. 2. Measurement of disc bulging with strain gauge.

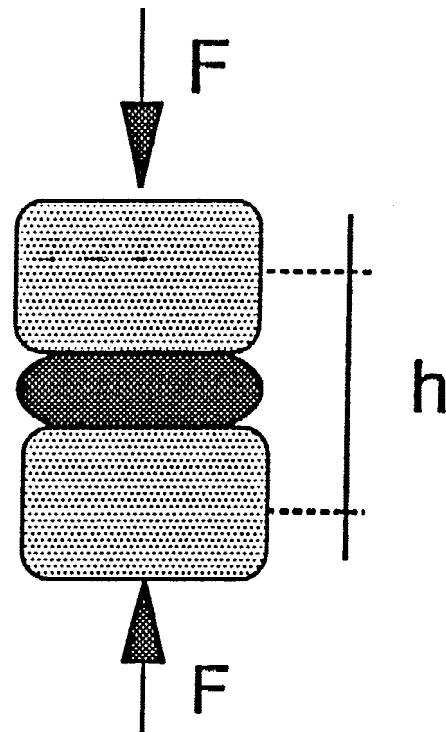


Fig. 3. Measurement of stiffness to a given axial deformation.

ence between the starting values before chemonucleolysis and lasernucleotomy. After setting the chemonucleolysis needle, an axial load of up to 400 Newton resulted in a bulging of $0.52 \text{ mm} \pm 0.32 \text{ mm}$, $0.49 \text{ mm} \pm 0.29 \text{ mm}$, and $0.28 \text{ mm} \pm 0.11 \text{ mm}$ as measured by the sensors 1, 2, and 3, respectively (Table 1). Statistical evaluation showed a significantly lower value ($P < 0.05$) for the measurement of sensor 3 in immediate vicinity of the chemonucleolysis needle. Equal axial load after setting of the laser trocar resulted in a bulging of $0.34 \text{ mm} \pm 0.08 \text{ mm}$, $0.29 \text{ mm} \pm 0.06 \text{ mm}$ and $0.10 \text{ mm} \pm 0.08 \text{ mm}$ as measured by the sensors 1, 2,

TABLE 1. Distribution of Bulging (in mm) Comparing Chemonucleolysis and Lasernucleotomy

	Preop.	P value	Postop
Sensor 1			
Laser	0.25 ± 0.1	n.s. ^a	0.28 ± 0.18
P value	n.s. ^a		n.s. ^a
Chemonucl.	0.28 ± 0.24	n.s. ^a	0.46 ± 0.42
Sensor 2			
Laser	0.22 ± 0.12	n.s. ^a	0.88 ± 0.38
P value	n.s. ^a		<0.05
Chemonucl.	0.21 ± 0.21	n.s. ^a	0.14 ± 0.08
Sensor 3			
Laser	0.12 ± 0.1	<0.05	0.22 ± 0.14
P value	n.s. ^a		0.05
Chemonucl.	0.21 ± 0.13	<0.05	0.12 ± 0.05

^an.s. = not significant.

and 3, respectively. In this case, too, there was a significant decrease ($P < 0.01$) in the vicinity of the trocar, as measured by sensor 3. Preoperative comparison of both methods showed a significantly decreased bulging after setting of the laser trocar (0.10 mm ± 0.08 mm vs. 0.28 mm ± 0.11 mm, $P < 0.01$). There was no significant difference in the stiffness of the disc ($\mu\text{m}/\text{N}$) after puncture with the different instruments (Laser nucl. 0.17 mm ± 0.04 mm vs. Chemonucl. 0.18 mm ± 0.15 mm).

Postoperative Bulging

After chemonucleolysis we found a decreased bulging within the dorsal areas of sensors 2 and 3 due to axial loading. However, the same measurements after laser therapy showed an equally distributed bulging in the ventral and dorsal sections. Comparison between pre- and postoperative values after chemonucleolysis exhibited a significantly decreased bulging at sensor 3 and an obvious, but not significant reduction in bulging at sensor 2 due to axial loading. After laser therapy we found a significantly increased bulging at sensor 3 and an insignificant increase at sensor 2 after axial loading (Table 1). In a direct postoperative comparison with chemonucleolysis, laser treatment exhibited significantly increased bulging. Whereas the stiffness of the disc decreased significantly with laser treatment, there was only a slight tendency toward decreased stiffness of the disc in chemonucleolysis (Table 2).

DISCUSSION

Chemonucleolysis with chymopapain is disputed because of its side effects, as anaphylaxis, neurologic complications up to transverse myeli-

TABLE 2. Comparison of Preoperative and Postoperative Ratio of Lateral Elasticity (per definition the reciprocal value of the stiffness) Against Axial Loading

	Preop. (N/ μm)	P value	Postop.
Laser	0.44 ± 0.1	<0.01	0.35 ± 0.08
P value	n.s. ^a		n.s. ^a
Chemonucl.	0.45 ± 0.38	n.s. ^a	0.39 ± 0.36

^an.s. = not significant

tis and back spasm [25,26], but represents an established method with clinical efficiency evidenced in double-blind studies [1,14,16]. Percutaneous lasernucleotomy is regarded as the latest semiinvasive method of treatment with encouraging results [6,8,11,12,19]. However, standardized comparative studies are still missing.

Intravital biomechanical investigations reported a definite reduction in intradiscal pressure brought about by injection of chymopapain [27]. Wakano et al. [22] found a decrease in stiffness of the disc 3 weeks postchemonucleolysis. Choy et al. [20] also reported a decrease in intradiscal pressure in laser-treated cadaver discs. They support the hypothesis that a sudden decrease in intradiscal pressure induced by laser evaporation of the nucleus might cause a retraction of the prolaps and thereby a relief of the nerve root [6]. Therefore, the present study was designed to compare for the first time the basic biomechanical effect of chemonucleolysis and lasernucleotomy on the dorsal outer circumference of the disc.

Proceeding on the assumption that pressure relief of the dural sack and the nerve root, respectively, is one of the determining factors for the success of a semiinvasive method of disc prolaps treatment [6,13,25,26,28,29], the relevant factor is not the intradiscal pressure, but the displacement of the disc at the dorsal circumference under increasing axial load. The publications by Hoppenfield [30] and Kambim and Brager [31] postulating an effect of fenestration of the annulus by the nucleotomy instruments caused us to check this effect by our experimental setup. Therefore, we measured the effects of the positioning of the nucleotomy instruments exerted on the circumferential displacement of the disc. Confirming this hypothesis, our results show a significantly lower bulging at the area of insertion of instruments. This phenomenon might be explained by a stabilizing effect by the setting of the instruments. It was most pronounced at sensor 3 in immediate vicinity of the setting instrument and de-

creased with increasing distance from it. Thus the highest bulging values were measured at the most distant sensor 1. The considerably large diameter of the laser trocar also might result in a higher mechanical stabilization of the anulus as compared to the thinner chemonucleolysis needle (2.0 mm diameter of the laser trocar vs. 1.0 mm diameter of the chemonucleolysis needle). However, in a previous group consisting of five discs, the measurement after removing either the trocar or the needle without treatment showed practically no differences (due to a reachable accuracy) to the measurement before setting the instruments. Posttherapeutic measurements mainly indicate a decreased dorsal bulging after chemonucleolysis and an increased dorsal bulging after lasernucleotomy.

With our experimental setup, we were able to show that—in healthy discs at least—chemonucleolysis and lasernucleotomy exert different effects on the circumference of the anulus. The results of our study demonstrate that intradiscal injection of chymopapain significantly decreases bulging. Other authors also report significantly reduced intradiscal pressure upon application of chymopapain [27]. Furthermore, our investigation shows that reduction of intradiscal pressure after chemonucleolysis is associated with an only minor decrease in stiffness of the disc. Despite the enzymatic processes, the nucleus preserved a residual axial stiffness and was able to absorb a certain amount of axial pressure. The essential effect of action was a decreased intradiscal pressure with a maintained loading capacity of the nucleus. The therapeutic effect of lasernucleotomy seemed to be basically different from that of chemonucleolysis. The vaporisation of the nucleus resulted in a significantly lower axial stiffness of the disc. Following lasernucleotomy, bulging was found to be significantly increased mainly within the dorsal region and axial load caused the dorsal deformation. The postulated decompressive effect of lasernucleotomy on diseased discs could not be confirmed by our experimental setup, because for reasons of availability and reproducibility, only healthy discs could be used. However, after laser therapy of prolapsed discs top loads within the prolapsed area may be distributed all over the circumference of the anulus, thereby avoiding or reducing top loads within this restricted area. The results of this study were obtained under in vitro conditions. In our opinion these results might serve as a biomechanical basis for principle action after lasernucleotomy and

chemonucleolysis on the outer circumference of the disc. Nevertheless, caution is required in extrapolating results obtained under laboratory conditions to the clinical setting. Therefore, further studies will be necessary to reveal a possible significance of these fundamental findings for clinical use.

REFERENCES

1. Fraser RD. Chymopapain for the treatment of intervertebral disc herniation: A preliminary report of a double-blind study. *Spine* 1982; 7:608–612.
2. Kornberg M. Automated percutaneous lumbar discectomy as treatment for lumbar disc disruption. *Spine* 1993; 18:395–397.
3. Onik G, Helms CA, Ginsburg L, Hoaglund FT, Morris J. Percutaneous lumbar discectomy using a new aspiration probe. *AJNR* 1985; 6:290–293.
4. Buchelt M, Kutschera HP, Katterschafka Th, Kiss H, Ullrich R. Erb:Yag and Hol:Yag laser ablation of meniscus and intervertebral discs. *Lasers Surg Med* 1992; 12:375–381.
5. Castro WHM, Halm H, Jerosch J, Schilgen M, Winkelmann W. Veränderungen der lumbalen Bandscheibe nach Anwendung des Holmium-YAG lasers. *Z Orthop* 1993; 131:610–614.
6. Choy DSJ, Ascher PW, Saddekni S, Alkaitis D, Liebler W, Hughes J, Diwan S, Altman P. Percutaneous laser disc decompression: A new therapeutic modality. *Spine* 1992; 17:949–956.
7. Cummings RS, Prodoehl JA, Hermantin FU, Rhodes A, Sherk HH. Laser ablation of intervertebral discs using the Nd:Yag 1.44 μm laser. *Spine* 1993; 7:37–40.
8. Juri H, Ascher PW, Lillo J. Lumbar disc nucleolysis by Nd:Yag laser radiation: An experimental comparative study. *Lasers Surg Med* 1988; 8:196–201.
9. Leu HJ, Imhoff A, Schreiber A. Percutane Nucleotomie und Diskoskopie. Erste Erfahrungen mit der Excimer Photoablation. In: Siebert WE, Wirth CJ, eds. "Laser in der Orthopädie." Stuttgart: Thieme, 1991, pp 155–163.
10. Sherk HH, Rhodes A, Black J, Prodoehl JA. Results of percutaneous lumbar discectomy with lasers. *Spine* 1993; 7:141–150.
11. Siebert WE, Wirth CJ. Experimental investigations on use of lasers on the intervertebral disc. In: Brock M, Mayer HM, eds. "Percutaneous Lumbar Discectomy." Berlin: Springer, 1989, pp 205–214.
12. Siebert W. Percutaneous laser disc decompression: The European experience. *Spine* 1993; 7:103–134.
13. Bitz DM, Lord LT. An evaluation of narrowing following intradiscal injection of chymopapain. *Clin Orthop* 1977; 129:191–195.
14. Dabezies EJ, Langford K, Morris J, Shields CB, Wilkonson HA. Safety and efficacy of chymopapain (Discase) in the treatment of sciatica due to a herniated nucleus pulposus: Results of a randomized double-blind study. *Spine* 1988; 13:561–565.
15. Garvin PJ, Jennings RB, Schmith L, et al. Chymopapain: A pharmacologic and toxicologic evaluation in experimental animals. *Clin Orthop* 1965; 41:204.
16. Javid MJ, Nordby EJ, Ford LT, et al. Safety and efficacy

- of chymopapain (Chymodiactin) in herniated nucleus pulposus with sciatica: Results of a randomized, double-blind study. *JAMA* 1983; 249:2489-2494.
17. Gunzburg R, Fraser RD, Moore R, Vernon-Roberts B. An experimental study comparing percutaneous discectomy with chemonucleolysis. *Spine* 1993; 18:218-226.
 18. Revel M, Payan C, Vallee C, et al. Automated percutaneous lumbar discectomy versus chemonucleolysis in the treatment of sciatica. *Spine* 1993; 18:1-7.
 19. Choy DSJ. Percutaneous laser disc decompression using the 1.06 and 1.32 μm Nd/Yag laser. *Spine* 1993; 7:41-48.
 20. Choy DSJ, Altman P. Fall of intradiscal pressure with laser ablation. *Spine* 1993; 7:23-30.
 21. Monteiro A, Lefevre R, Pieter SG. Lateral decompression of a pathologic disc in the treatment of lumbar pain and sciatica. *Clin Orthop* 1989; 238:56-63.
 22. Wakano K, Kasman R, Chao EY, et al. Biomechanical analysis of canine intervertebral discs after chymopapain injection, preliminary report. *Spine* 1983; 8:59-68.
 23. Onik G, Maroon J, Helms C, Schweigel J, Mooney V, Kahanovitz N, Day A, Morris J, McCulloch JA, Reicher M. Automated percutaneous discectomy: Initial patients experience. *Radiology* 1987; 162:129-132.
 24. McCulloch JA, Macnab I. "Sciatica and Chymopapain." Baltimore: Williams & Wilkins, 1983.
 25. Davis RJ, North RB, Campbell JA, et al. Multiple cerebral hemorrhages following chymopapain chemonucleolysis: Case report. *J Neurosurg* 1984; 61:169-171.
 26. Dyck P. Paraplegia following chemonucleolysis: A case report and discussion of neurotoxicity. *Spine* 1985; 10:359-362.
 27. Takahashi K, Inoue S, Takada S, Nishiyama H, Mimura M, Wada Y. Experimental study on chemonucleolysis. *Spine* 1986; 11:617-620.
 28. Gibson MJ, Buckely J, Mulholland RC, Worthington BS. The changes in the intervertebral disc after chemonucleolysis demonstrated by Magnetic Resonance Imaging. *J Bone Joint Surg* 1986; 68B:719-723.
 29. Konings JG, Williams FJB, Deutman R. The effects of chemonucleolysis as demonstrated by computerized tomography. *J Bone Joint Surg* 1984; 66B:417-421.
 30. Hoppenfield S. Percutaneous removal of herniated lumbar discs. *Clin Orthop* 1989; 238:92-97.
 31. Kambin P, Brager MD. Percutaneous posterolateral discectomy, anatomy and mechanism. *Clin Orthop* 1987; 223:145-154.